ORIGINAL PAPER



# Strontium delivery systems based on bacterial cellulose and hydroxyapatite for guided bone regeneration

Erika Patricia Chagas Gomes Luz · Maria de Fátima Borges · Fabia Karine Andrade · Morsyleide de Freitas Rosa · Antonia Infantes-Molina · Enrique Rodríguez-Castellón · Rodrigo Silveira Vieira

Received: 6 February 2018/Accepted: 20 August 2018/Published online: 29 August 2018 © Springer Nature B.V. 2018

**Abstract** Hybrid materials (HMs) based on a combination of bacterial cellulose (BC) and hydroxyapatite (HA) have demonstrated promising capabilities, especially for bone repair. The insertion of strontium into a BC/HA matrix has a role in the body related to bone remodeling. This study aimed to obtain HMs containing BC/HA doped with strontium ions ( $Sr^{2+}$ ) by two routes of synthesis, differing in the way strontium was inserted. The HMs produced were characterized to elucidate the morphology and metal/ biopolymer interaction, and also strontium adsorption/ desorption profiles were evaluated. The biomaterials produced were able to interact with  $Sr^{2+}$ , showing a distinct adsorption/desorption profile for each

material. BC/CaHA/Sr showed an ion exchange between Ca<sup>2+</sup> present in hydroxyapatite by the Sr<sup>2+</sup> in solution, characterized by mainly a physisorption mechanism. BC/SrAp demonstrated a chemical bond of Sr<sup>2+</sup> on the BC surface by a chemisorption mechanism. The desorption study showed that the Sr release reached a plateau after 11 and 60 days and after 4 months, 91 and 6% of the adsorbed Sr<sup>2+</sup> was released by BC/CaHA/Sr and BC/SrAp, respectively. These results suggest that the delivery of Sr<sup>2+</sup> can be modulated during bone repair depending on the way Sr<sup>2+</sup> is inserted into the hybrid matrix.

E. P. C. G. Luz · F. K. Andrade · R. S. Vieira (⊠) Department of Chemical Engineering, Federal University of Ceará (UFC), Bloco 709, Fortaleza, Ceará 60455-760, Brazil e-mail: rodrigogpsa@gmail.com

M. F. Borges · F. K. Andrade · M. F. Rosa Embrapa Agroindústria Tropical–CNPAT, Rua Dra Sara Mesquita 2270, Pici, Fortaleza, Ceará 60511-110, Brazil

A. Infantes-Molina · E. Rodríguez-Castellón Departamento de Química Inorgánica, Facultad de Ciencias (Unidad Asociada al ICP-CSIC), Universidad de Málaga, 29071 Málaga, Spain



**Keywords** Biomaterials · Bone repair · Release systems · Bone tissue

#### Introduction

Guided bone regeneration is a method successfully employed in dental practices to increase the volume of the host bone at sites with insufficient bone quantity. Thus, before the dental implants can be surgically anchored into the jawbone via titanium screws, the reconstruction of deficient alveolar ridges is necessary to facilitate implant placement. For that, oral surgeons fill the socket with bone graft (allograft bone chips or ceramic particles) to stimulate new bone growth. To ensure the graft stays in place, the site is typically covered with a membrane, however the particles from the traditional bone grafts frequently leak and migrate, which could damage the surrounding soft tissues (e.g. gingiva, nerves, and sinus membranes; Hutchens 2007). Besides avoiding the migration of the allograft bone chips or ceramic particles, this membrane barrier is used in guided bone regeneration (GBR) to protect the defect area against the invasion of non-osteogenic tissues that have a higher migration velocity than osteogenic cells. Membrane barriers must have characteristics that lead to biological, mechanical and clinical use requirements to serve as a barrier against unwanted cell invasion since these cells inhibit bone formation and stimulate the down-growth of the connective tissue into the area of injured tissue (Rad et al. 2017). Some of the indispensable requirements to act as a passive physical barrier are: biocompatibility, cell occlusion properties, capacity to create a secluded space, tissue integration and be clinically handled. Moreover, clinical reports found in the literature show that both absorbable and nonabsorbable membranes are effective in the process of guided bone regeneration, provided that an adequate technical protocol is applied in each case, in order to minimize complications (Rakhmatia et al. 2013; Retzepi and Donos 2010).

Hybrid materials (HM) obtained from bacterial cellulose (BC) and hydroxyapatite (HA) have been shown to be promising materials for use in guided bone regeneration (GBR) (Grande et al. 2009; Saska et al. 2011), since BC is a biopolymer with excellent biocompatibility, high mechanical properties, high crystallinity, and high water retention capacity (Ahn et al. 2015; Duarte et al. 2015; Pértile et al. 2012; Rajwade et al. 2015) while HA is a ceramic that naturally constitutes bones and teeth and has high biocompatibility, stability at physiological pH, and stimulates osteointegration (Pigossi et al. 2015). One advantage of using BC/CaHA hybrids is that, since the HA particles are physically bound to cellulose fibers, this type of system prevents the HA particles from migrating to neighboring areas, which avoids damage of the surrounding soft tissues, making the application of an extra membrane to cover the graft unnecessary (Hutchens 2007).

Recently, our group synthesized a biocompatible biomaterial based on BC and hydroxyapatite. In this case, a calcium-deficient apatite, which is similar to biological apatites, was deposited on the cellulose fibers. The biocomposite presented in vitro bioactivity and was suitable for the preparation of nanocomposites for applications in the regeneration of bone tissue (Duarte et al. 2015).

In this sense, in the present work, aiming to enhance the benefits of BC/HA composites in promoting bone remodeling mechanisms, strontium ions  $(Sr^{2+})$  were incorporated into this hybrid material. Literature relates that preclinical studies demonstrated strontium action mechanisms on bone modeling and confirmed its role as an inhibitor of bone reabsorption, reducing the activity of osteoclasts (Schumacher et al. 2016) while at the same time inducing bone formation by stimulating osteoblast activity (Marie et al. 2010; Zhang et al. 2011). Its dual action is related to its chemical similarity to calcium (Querido et al. 2016). Calcium is a necessary nutrient for the functioning of the human body, since it is involved in many reactions, such as bone formation, muscle contraction, enzyme activation, cell differentiation, programmed cell death, and neuronal activity (Chen et al. 2012; Wang et al. 2009; Zhang et al. 2014; Zhong et al. 2013; Zhou et al. 2012).

In the present study, bacterial cellulose/hydroxyapatite hybrids functionalized with strontium ions were characterized in relation to their chemical structure, morphology, porosity, surface composition, their power of swelling degree and their capacity of adsorption and desorption. The adsorption/desorption of  $\mathrm{Sr}^{2+}$  by the HM was also evaluated in order to know the delivery rate of this metal ion and to elucidate the metal/biopolymer interaction.

#### Materials and methods

#### Reagents and media components

Bacteriological agar, casein peptone, and yeast extract powder were purchased from  $\text{Difco}^{\text{TM}}$  (Detroit, Michigan, USA). Citric acid hydrate, d(+) glucose anhydrous, sodium dihydrogen phosphate anhydrous,

and sodium hydroxide and were purchased from Sigma-Aldrich (St. Louis, Missouri, USA).

#### Microorganism and media preparation

*Komagataeibacter hansenii* ATCC 23769 strain was used as the BC-producing bacterial source. The strain was previously stored at -18 °C in mannitol broth (5.0 g/L of yeast extract; 3.0 g/L of peptone, and 2.5 g/L of d-mannitol) containing 20% glycerol (w/v). The activation was performed in mannitol broth and the bacteria was cultured statically at 30 °C for 2 days. The culture was propagated by inoculation of 3% (v/v) from mannitol broth to HS medium (Hestrin and Schramm 1954) at 30 °C for 48 h. Finally, the inoculum was added to Falcon tubes containing 20 mL HS media and incubated at 30 °C for 6 days. The BC pellicles were purified with 2% sodium hydroxide and sterilized by exposure to 121 °C for 30 min.

#### Hybrid production

In this present study, bacterial cellulose/hydroxyapatite hybrids functionalized with strontium ions were synthesized by two different routes. For the synthesis of the first hybrid, the hybrid (BC/CaHA) was produced followed by its immersion in strontium nitrate solution to promote the exchange of calcium ions by strontium ions. For the synthesis of the second hybrid, the strontium ions were directly introduced into the BC matrix leading to the precipitation of strontium apatite on the BC fibers.

The first route was conducted as proposed by Hutchens et al. (2006) and is described as follows: After purification, the BC pellicles (25 mm) were immersed in 25 mL CaCl<sub>2</sub> solution (11.1 g/L) and mildly stirred at 25 °C for 24 h. Thereafter, for the removal of CaCl<sub>2</sub> excess, the pellicles were washed with deionized water, followed by immersion in 25 mL of Na<sub>2</sub>HPO<sub>4</sub> solution (8.52 g/L) using the same conditions previously described. This alternate soaking process (immersion in calcium and phosphate solutions) was repeated three times with the samples rinsed thoroughly with deionized water between each soaking cycle (  $\sim 10$  mL of deionized water for 3 min at 25 °C). Finally, the composite BC/CaHA was removed and freeze-dried. For incorporation of strontium, the BC/CaHA composite was immersed in

strontium nitrate solution (100 mg/L) at 40  $^{\circ}$ C for 2 h leading to the production of the BC/CaHA/Sr hybrid.

For the second method, strontium hydroxyapatite was directly deposited onto the BC fibers to produce the BC/SrAp hybrid according to the methodology described by Hutchens et al. (2006) with adaptation. For this, alternate soaking of BC pellicles in 25 mL of SrCl<sub>2</sub> solution (100 or 1000 mg/L) and Na<sub>2</sub>HPO<sub>4</sub> solution (8.52 g/L) under gentle agitation at 25 °C for 24 h was performed. This process was repeated five times with the samples rinsed thoroughly with deionized water between each soaking cycle ( $\sim$  10 mL of deionized water for 3 min at 25 °C), and the BC/SrAp was freeze-dried. To evaluate the Sr<sup>2+</sup> incorporation into the hybrid matrix after each cycle, aliquots from the aqueous phase were taken and analyzed by atomic absorption spectrometry (AAS).

## Swelling degree and porosity

The swelling degree was assessed using the method described by Liu et al. (2005). The hybrids produced were immersed in phosphate buffered saline (PBS) at pH 7.4 during intervals of 0, 1, 2, 7, 12, 22, 32, 52, and 72 min at 25 °C. After each immersion, the excess buffer was removed with filter paper and the pellicle was weighed. The porosity of the hybrids was obtained as described by Zeng and Ruckenstein (1996). Porosity was determined by considering the amount of water inside the pores, taking in account the weight of the wet and dry (lyophilized) sample.

The swelling degree (SD) was expressed as the percentage of weight increase compared to the initial weight, as described in Eq. 1:

$$SD = (W_s - W_d/W_d) \times 100 \tag{1}$$

The porosity ( $\epsilon$ ) is estimated by Eqs. 2 and 3.

$$\epsilon(\%) = \{ (W_s - W_d) / \rho_{water} \} \times 100/v$$
(2)

$$\mathbf{v} = (\pi \mathbf{D}^2 \mathbf{h})/4 \tag{3}$$

where  $W_s$  is the weight of the sample after immersion, and  $W_d$  is the weight of the dry sample before immersion,  $\epsilon$  is the porosity of the membrane and  $\rho_{water}$  is the specific mass of water at 20 °C, v is volume of the pellicle, D is the diameter and h is the height. Scanning electron microscopy (SEM) and energydispersive X-ray spectroscopy (EDX)

Before SEM and EDX analyses the lyophilized samples were placed in a stub and sputter-coated with gold. The SEM images were obtained with a DSM 940A scanning electron microscope (SEM; Zeiss, Germany) with an acceleration voltage of 15 kV. EDX analyses were obtained using an Inspect S50 scanning electron microscope (FEI, Hillsboro, Oregon, USA) with an acceleration voltage of 10 kV.

# N<sub>2</sub>-adsorption isotherms

The surface area and the pore diameter of the samples were experimentally determined by nitrogen adsorption/desorption isotherms at -196 °C using a Micromeritics ASAP 2020 analyzer. The samples were previously degassed at 200 °C in a vacuum of  $10^{-5}$  bar. The textural properties were calculated according the BET technique (Brunauer et al. 1938).

# Fourier-transform infrared spectroscopy (FTIR)

The FTIR spectrum analysis was conducted to confirm the functional groups in the hybrid materials. Samples were examined using an FTLA 2000-102 (ABB-BOMEM) spectrophotometer equipped with an attenuated total reflectance (ATR) accessory. Spectra were obtained between 4000 and 400 cm<sup>-1</sup> at a resolution of 4 cm<sup>-1</sup> over 25 scans.

Solid state nuclear magnetic resonance (NMR)

<sup>31</sup>P and <sup>13</sup>C MAS NMR spectra were recorded at room temperature with a Bruker AVANCEIII HD 600 spectrometer using an HXY, Efree MAS probe of 3.2 mm at a spinning rate of 15 kHz. The magnetic field was 14.1 T corresponding to <sup>13</sup>C and <sup>31</sup>P resonance frequencies of 150.9 and 242.9 MHz, respectively. All spectra were recorded using a CP-MAS pulse program: a combination of cross-polarization, high-power proton decoupling, and magic angle spinning. The <sup>13</sup>C chemical shift values were measured with respect to glycine as a secondary reference (carbonyl signal at 176.03 ppm) and <sup>31</sup>P with respect to ammonium dihydrogen phosphate at 0.9 ppm.

#### X-ray photoelectron spectroscopy (XPS)

X-ray photoelectron spectra were collected using a Physical Electronics PHI 5700 spectrometer with nonmonochromatic MgK $\alpha$  radiation (300 W, 15 kV, and 1253.6 eV) with a multi-channel detector. Spectra were recorded in the constant pass energy mode at 29.35 eV, using a 720 µm diameter analysis area. Charge referencing was measured against adventitious carbon (C 1 s at 284.8 eV). A PHI ACCESS ESCA-V6.0 F software package was used for acquisition and data analysis. A Shirley-type background was subtracted from the signals. Recorded spectra were always fitted using Gaussian–Lorentzian curves in order to determine the binding energy of the different element core levels more accurately.

#### Adsorption studies with the hybrid BC/CaHA/Sr

#### Adsorption kinetics of Sr ions

Batch experimental studies were carried out with a fixed mass (0.035 g of dry weight) of adsorbent in strontium nitrate solution of 100 mg/L, under controlled temperature conditions at 25 °C and pH 6.0. BC/CaHA pellicles were immersed in Sr solutions and agitated using rotary shaker tubes (TE-165 TECNAL) at 45 rpm. At intervals of 0.25, 0.5, 1, 2, and 3 h, the adsorbent was removed and the aqueous-phase concentration of the metal was determined with an atomic absorption spectrophotometer (AA240FS FAST sequential atomic absorption spectrometer).

#### Effect of pH

The effect of pH on adsorption of  $\text{Sr}^{2+}$  was evaluated. The experiments were conducted in batch mode using a fixed mass of the adsorbent (0.035 g of dry weight) immersed in strontium nitrate solutions (100 mg/L) at pH values ranging from 2.0 to 6.0 at room temperature for 2 h. The pH of the solution was adjusted using 0.1 M NaOH and 0.1 M HCl.

#### Temperature effect on Sr adsorption

To study the influence of temperature on the adsorption of Sr ions by the BC/CaHA hybrid, strontium nitrate solutions were prepared at a concentration of 100 mg/L at pH 6.0, using a fixed mass of the adsorbent (0.035 g of dry weight) for a period of 2 h. The experiments were performed at temperatures of 20, 25, 30, and 40  $^{\circ}$ C.

#### Adsorption isotherm

Adsorption isotherms were performed in a batch system using 0.035 g of adsorbent in 25 mL of strontium nitrate solution at a concentration range of 10–350 mg/L, at pH 6.0. A thermostatic bath at 25 °C or 40 °C under constant stirring (150 rpm) was used. After 2 h, the adsorbent was removed and the aqueous-phase concentration of metal was determined by atomic absorption spectrometry (AAS) at a wavelength of 460 nm. In order to increase the analysis sensitivity as air-acetylene gas was used, 2 mL of chloride potassium solution (10.000 mg/L) and 0.2 mL of 50% lanthanum were added to eliminate any interference, to each 10 mL sample.

#### Sr desorption studies

The desorption profiles of Sr ions from the two hybrid materials were evaluated in order to determine the  $Sr^{2+}$  delivery rate and elucidate metal/adsorbent interactions. Experiments to measure the amount of strontium desorbed were performed by immersing 0.035 g of dry weight of the hybrid sample in 10 mL of phosphate buffered saline (PBS) at pH 7.4, 37 °C under stirring (150 rpm). At each time studied, an aliquot of 3 mL was collected, the remaining volume of the buffer was discarded, and finally 10 mL of fresh PBS was added. Aliquots from each time point were analyzed by AAS to quantify the amount of strontium desorbed.

#### **Results and discussion**

#### Swelling degree

The main mechanisms that influence the swelling are the diffusion of the penetrating solvent and polymer stability (Capitani et al. 2001). This process is of considerable importance and allows for determination of the interaction of the material with solvents.

The swelling of the hybrid materials occurred rapidly, indicating that its structure facilitated water penetration, allowing interaction with the polymer matrix. The BC/SrAp hybrid obtained the highest swelling degree of 1019  $\pm$  0.03%, followed by BC/CaHA/Sr (961  $\pm$  0.13%) and BC/CaHA (894  $\pm$  0.05%) (Fig. 1).

These results suggest that there are hydrophilic groups available in the polymer structure, with different levels of hydrophilicity, and they are related to the water affinity of the groups of the polymer and apatite. The Sr insertion in the composite matrix lead to solubility of some of the deposited apatite, which was in agreement with the study of Pan et al. (2009) which showed the solubility isotherms of partially and fully substituted strontium hydroxyapatite. The increase in solubility with higher strontium content was interpreted as a destabilization of the crystal structure by the larger strontium ion.

From the swelling test it was possible to estimate the porosity of the materials using both the dry and wet weights. Membranes used in GBR should allow the diffusion of interstitial fluid, at the same time that inhibits the invasion of cells from connective and epithelial tissue (Retzepi and Donos 2010). Transport of oxygen and nutrients and metabolic waste removal through the membrane is mainly a function of diffusion, which is governed by its porosity and permeability. Moreover, high porosity provides more sites for the binding of a delivered compound (e.g., strontium metal ions).

The BC/CaHA presented a large volume of pores corresponding to 83%, which favors strontium adsorption, facilitating the interaction between adsorbate and adsorbent. However, after the immersion of BC/CaHA in strontium nitrate solution for the production of the functionalized BC/CaHA/Sr hybrid, the porosity decreased to 72%. The BC/SrAp hybrid presented a porosity of 84%, similar to BC/CaHA. For nonresorbable membrane (e.g., BC implants), there is a general consensus that implant porosity should be above 60%, as below this value sustainable bone integration into the central pore chambers cannot be expected (Hing 2005).

# Scanning electron microscopy (SEM)

The morphology of raw bacterial cellulose fibers is shown in Fig. 2a. The BC network includes nanofibrils (the width of the fibers is in the nanometer range) and is considered highly porous (Fig. 2a). This type of 3D structure makes BC an outstanding material for drug transfer and as a physical barrier, and in the last several decades it has been used as a wound dressing and for bone regeneration (Zimmermann et al. 2011).

In Fig. 2b, it is possible to observe the morphology of the BC/CaHA matrix. After the deposition of hydroxyapatite through immersion cycles in calcium and phosphate solutions, the BC surface was completely covered by globular crystallites typical of calcium apatite, as described by other authors (Duarte et al. 2015).

The structure found in Fig. 2c showed that after the BC/CaHA was immersed in strontium nitrate solution in order to incorporate this metal in the matrix of the hybrid material some hydroxyapatite crystals present on the surface of the composite seemed to dissolve in the aqueous phase. BC fibers between crystallites became exposed and could be visualized, which corroborates the porosity and swelling degree results.

Figure 2d shows that the apatite formed on BC fibers from strontium phosphate solution is morphologically similar to the hydroxyapatite formed from calcium phosphate solution (Fig. 2b). Melnikov and Gonçalves (2015) synthesized and characterized strontium hydroxyapatite ( $Sr_{10}(PO_4)_6(OH)_2 \cdot 10H_2O$ ) for orthopedic applications. The morphological analyses by SEM of SrAp samples showed that the crystals formed at room temperature were tiny irregular granules of around 5 nm in diameter. However, with the increase in temperature, the granules increased in size and exhibited star-like aggregates composed of a mean needle length of 5100 nm and a diameter of 340 nm.

# N2-Adsorption/desorption isotherms

The textural properties, such as surface area and pore diameter, are relevant to determine the accessibility of the adsorption sites. The specific surface area, average pore diameter, and specific volume of the pores of the materials were determined by the BET method, and the results obtained are shown in Table 1.

The nitrogen adsorption isotherms at -196 °C for BC, BC/CaHA, BC/CaHA/Sr, and BC/SrAp samples present a type IV profile with H3 hysteresis, which is a characteristic of mesoporous materials (pore sizes of 2–50 nm), according to IUPAC classification. These isotherms present an adsorption curve that does not overlap the nitrogen desorption curve, which is associated with the phenomenon of capillary

condensation, where saturation pressures are not equal inside the pores, causing hysteresis (Ceratti et al. 2015).

The results presented in Table 1 indicate that the measurements of the surface area properties, specific pore volume, and average pore diameter increased after the interaction of BC with calcium HA. The literature reports that HA is an inorganic solid that has a surface area around 48 m<sup>2</sup>/g (Venugopal and Scurrell 2003) which is larger than the BC surface area, indicating the benefit of BC and HA interaction. Moreover, the HMs presented pore sizes less than 25 nm. It is know that a pore size  $< 1 \mu m$  results in a larger surface area that is believed to contribute to the bioactivity and bone-inducing protein adsorption (Vallet-Regí and Ruiz-Hernández 2011). In general, these hybrid membranes are an highly porous material, which facilitates the adsorption of strontium (as it will be showed in next sections) and probably also the passage of interstitial fluids and oxygen. In addition, due to the small pore sizes, will also act as a barrier preventing the invasion of non-osteogenic cells in the region that it is intended to promote bone repair.

Comparing the average pore diameter of BC/CaHA with BC/CaHA/Sr and BC/SrAp hybrids, the decrease was probably because of the insertion of the strontium metal in its structure. This result is related with the swelling and porosity results, which is evidenced by some solubilization of the HA matrix.



Fig. 1 Swelling degree of hybrid materials produced in PBS buffer at pH 7.4. BC/CaHA/Sr (■), BC/SrAp (●) and BC/CaHA (♦)

Fourier-transform infrared spectroscopy (FTIR)

The infrared analyses were performed in order to characterize the functional groups presented in each hybrid material.

The FTIR spectra of the hybrid materials are displayed in Fig. 3, and the band assignments are summarized in Table 2 In the vibrational spectra of native BC, typical vibration bands of the cellulose structure appeared at 3350 cm<sup>-1</sup> (O-H bond stretching), 2900-2850 cm<sup>-1</sup> (stretching of CH and asymmetric stretching of  $CH_2$ ), 1426 cm<sup>-1</sup> (asymmetric angular deformation of C–H bonds), 1360-1378 cm<sup>-1</sup> (symmetric angular deformation of C-H bonds), 1060 cm<sup>-1</sup> (asymmetrical stretching of C–O–C glycosidic bonds), and 107–1055 cm<sup>-1</sup> (stretching of C– OH and C-C-OH bonds for secondary and primary alcohols, respectively). We also observed bands corresponding to C-H bond bending or CH<sub>2</sub> stretching at 900 cm<sup>-1</sup>, as well as O-H out-of-plane bending at  $665 \text{ cm}^{-1}$  (Dufresne 2012; Gea et al. 2011; Ummartyotin et al. 2017).

The vibrational spectra of all three hybrids (Fig. 3), absorption did not show the bands at 2919–2850 cm<sup>-1</sup>, commonly found in BC, probably because of the intense absorption by the structural skeleton of apatite. Bands related to phosphate groups were present only in the vibrational spectra of BC/ CaHA and BC/SrAp at the same time that the band around 1400 cm<sup>-1</sup> was only found in BC/CaHA/Sr and native BC. These observations corroborate the observation obtained by SEM results, which showed that after the BC/CaHA was immersed in strontium nitrate solution, some of the hydroxyapatite crystals present on the surface of the composite were dissolved to the aqueous phase, thus exposing the network of cellulose fibers.

These results are confirmed by NMR, since it indicates that the samples show characteristics of cellulose due to the presence of the basic unit, glucose. It also indicates that the formation of hybrids results from the interaction of Ca, Sr, and P with hydroxyl groups, showing a preferential substitution in this position.

#### Solid state NMR spectroscopy

<sup>13</sup>C CP-MAS profiles (Fig. 4) show the characteristic peaks of cellulose. In general, it is clearly observed a

Fig. 2 Electron micrographs of the surfaces from raw bacterial cellulose (a), and the hybrid materials BC/CaHA (b), BC/CaHA/Sr (c), and BC/SrAp (d)



decrease in the relative intensity of all resonance signals after the inorganic inclusion. If the spectra are compared, the peaks in the range of 60–105 ppm associated with anhydrous glucose units (Heinze et al. 2014; Foresti et al. 2017) are those affected by Ca, Sr and P insertion. The signal corresponding to C6 carbon bearing OH groups changes shifting at higher values, indicating a preferential substitution in that position (Fig. 4).

<sup>31</sup>P CP-MAS analysis confirmed that phosphate groups are chemically bonded to the material. The sample without Sr, BC/CaHA, shows three main contributions located at 1.4, -0.3 and -2.0 ppm. These values are close to those reported in literature for PO<sub>4</sub><sup>3-</sup>, HPO<sub>4</sub><sup>2-</sup> and H<sub>2</sub>PO<sub>4</sub><sup>-</sup> ions, respectively (Lin et al. 2005). After Sr incorporation into this material, the main signal observed was that at 1.4 ppm, indicating that  $PO_4^{3-}$  ions are those present in this sample. Moreover, a small contribution at 4.5 ppm could be due to isolated  $PO_4^{3-}$  units (Lin et al. 2005). The spectrum for BC/SrAp is again different. <sup>31</sup>P chemical shift for Sr hydroxyapatite is reported at 2.2 ppm (Sugiyama 2003) and could correspond to the band at 1.7 ppm. However, the most important contributions are located between -2.4 and -3.4 ppm. That could correspond to Sr-type phosphate without apatite structure. Previous studies reveal that Sr retards apatite-like phase formation (Henderson et al. 2016). By comparing all the spectra, it is clearly observed that after Sr incorporation into BC/CaHA, it is observed only one type of phosphate, pointing to a cationic H-Sr exchange and indicating that Sr is incorporated in the  $HPO_4^{2-}$  and  $H_2PO_4^{-}$ groups of BC/CaHA sample. These results indicate

Sample	Specific surface area (m <sup>2</sup> /g)	Specific volume of pores (cm <sup>3</sup> /g)	Average pore diameter (nm)		
BC	22	0.102	18.3		
BC/CaHA	59	0.354	24		
BC/CaHA/Sr	36	0.118	12.8		
BC/SrAp	86	0.287	13.2		

Table 1 Textural properties of BC, BC/CaHA, BC/CaHA/Sr, and BC/SrAp obtained through the nitrogen adsorption/desorption isotherms

different chemical coordination of Sr with and without calcium. In the former case, Sr is forming a hydroxyapatite structure, but in the latter case, Sr-type phosphate, without apatite structure is also present and could play an important role in the Sr-release process.

The surface composition of these materials was evaluated by means of X-ray photoelectron spectroscopy. C 1s, O 1s, P 2p, Ca 2p, Sr 3p, Na 1s, N 1s core level signals were studied.

Considering C 1s spectra (Fig. 5), in all cases three main signals are evidenced at 284.8, 286.4, and 288.1 eV. The first one is assigned to adventitious carbon from surface contamination. The second one at 286.6 eV is the main peak of cellulose, and assigned to C–O in alcohol and ether groups; the third one (blue contribution) is attributed to acetal moieties (O–C–O and/or C = O) (Khiari et al. 2017). The chemical shifts relative to C signal of adventitious carbon were  $1.7 \pm 0.1$  and  $3.1 \pm 0.1$  eV, as reported in literature (Dolinina et al. 2017). If the spectra are compared, BC contributions are less evident in the case of BC/CaHA indicating that the incorporation of CaHA takes place



Fig. 3 Vibrational spectra in the infrared region of the hybrid materials BC, BC/CaHA, BC/CaHA/Sr, and BC/SrAp

homogenously on the BC surface. Instead, when BC/ CaHA is immersed in a strontium nitrate solution to form BC/CaHA, some hydroxyapatite is dissolved and the two C 1s peaks arising from BC are much more pronounced confirming what was observed before with other techniques, i.e., some network of cellulose fibres are exposed on the surface.

Considering the O 1s signals, in the case of BC sample only one peak is noticeable at 532.8 eV. This binding energy value is similar to that found in literature for cellulose (Dolinina et al. 2017). The signal is broad and should include O-C-O and/or C = O and OH groups. The incorporation of apatites generates a new O 1s contribution at ca. 531.1 eV (green contribution) attributed to the corresponding phosphate groups (Hidalgo-Carrillo et al. 2012). As observed in the case of C 1s signal, O contribution due to cellulose is less important than that of phosphate in the case of BC/CaHA (See Table 3), but become more important after Sr incorporation. Moreover, in accordance to C 1s signal, in BC/SrAp the contributions of BC are more important indicating that it has not been achieved a homogeneous distribution of SrAp on the BC surface and some parts of cellulose are exposed on the surface.

Considering the phosphorous signal (Fig. 6), P 2*p* signal is that much more sensitive to oxidation states; however, P 2*p* signal for Sr containing samples overlaps with Sr 3*d* core level signal, therefore P 2*s* spectra have been considered in these two cases, although it is less sensitive to distinguish different oxidation states. BC/CaHA sample exhibits a main P 2*p*<sub>3/2</sub> peak (solid line) at 132.7 eV, which is ascribed to phosphate groups in apatites (Hidalgo-Carrillo et al. 2010; Ohtsu et al. 2012). In the case of samples containing Sr, P 2*s* spectra showed in both cases a main signal centered at ca. 190.5 eV, the values reported for HA samples (Shpak et al. 2004). No major

Table 2Assignments ofFTIR spectra of hybrid	Wavenumber (cm <sup>-1</sup> )	Band assignments <sup>a</sup>		
materials	3500 (BC/CaHA, BC/SrAp, BC/CaHA/Sr)	Stretching of OH groups		
	1653 (BC/CaHA, BC/SrAp, BC/CaHA/Sr)	OH angular deformation of adsorbed water		
	1430 (BC/CaHA/Sr)	Angular deformation of CH <sub>2</sub>		
	1387 (BC/CaHA/Sr)	Angular deformation of CH <sub>3</sub>		
	1100, 1033, 950 (BC/CaHA, BC/SrAp)	Asymmetric deformation of the PO <sub>4</sub> <sup>3-</sup> group		
<sup>a</sup> Bhatnagar (1967),	864 (BC/CaHA); 745 (BC/SrAp)	P–O(H) stretching		
Cacicedo et al. (2016),	610 (BC/CaHA, BC/SrAp)	Angular deformation of phosphate groups		
Rehman and Bonfield (1997), Yukhnevich (1973)	560 (BC/CaHA, BC/SrAp, BC/CaHA/Sr)	Asymmetric deformation of P-O(H)		

changes were observed in the position of this band, although was less intense in the case BC/SrAp sample.

Considering Ca 2p spectra (Fig. 7), it is shown two peaks ascribed to the Ca  $2p_{3/2}$ -Ca  $2p_{1/2}$  spin orbit doublet, and the binding energy of Ca  $2p_{3/2}$  component centered in both cases to ca. 347.3 eV, also consistent with that reported in the literature for apatites (Ide-Ektessabi et al. 2005; Hidalgo-Carrillo et al. 2012). The contribution of this signal is much lower in the case of BC/CaHA/Sr compound, as expected due to the incorporation of Sr and the loss of some calcium apatite during synthesis as exposed above. The N 1s signal is centered at 399.6 eV, which could be due to some remaining amides on the surface. No major changes were observed among the samples. Na 1s signal is located at 1071.3 eV, typical of sodium phosphates such as Na<sub>2</sub>HPO<sub>4</sub> and Na<sub>3</sub>PO<sub>4</sub> species (Swift 1982).

The corresponding surface atomic composition is included in Table 3.

As observed from this Table 3, the amount of P and Ca present on the surface decreases after Sr insertion. In the case of BC/SrAp sample, a greater surface Sr exposure is present and explains the lower amount of P detected on the surface.

From these results it is observed a different surface distribution depending on the sample composition. Thus the sample without Sr shows an homogeneous distribution of CaHA on the surface, although after Sr incorporation part of it is dissolved and BC is exposed on the surface. The sample without Ca, BC/SrAp, shows a surface enrichment of Sr and according to NMR results part of Sr is forming Sr-phosphate without HA structure.



Adsorption studies with the hybrid BC/CaHA/Sr

#### Kinetics of adsorption of Sr ions

The adsorption kinetics were assessed in order to determine the optimum adsorption time of Sr ions by the hybrid BC/CaHA. Sr<sup>2+</sup> adsorption occurred mainly on the material surface and the adsorbed amount was 17.22 mg of Sr per gram of adsorbent. The amount of  $Sr^{2+}$  increased rapidly in the first hour and thereafter increased slowly. The equilibrium time, at which adsorption of Sr ions by the hybrid BC/CaHA became constant, was reached after 2 h (Fig. 8), indicating that the active sites were completely occupied and showed favorable adsorption kinetics.

Wang et al. (2009) studied the adsorption behavior of Sr<sup>2+</sup> on gels from several polysaccharide derivatives, including carboxymethylcellulose (CMC). The authors found that the equilibrium time for Sr adsorption on CMC was reached at 1 h. In this case, the material showed an adsorption of 99 mg per g of gel with Lagmuir adjustment, which can be explained by ion exchange mechanisms.

Chen et al. (2009) compared the adsorption of copper and lead ions by pure BC membranes and BC membranes containing carboxymethylcellulose (CMC). The adsorption capacity of metal ions by BC membranes containing CMC (12.63 mg Cu/g and 60.42 mg Pb/g) was higher than that of pure BC membranes (9.67 mg Cu/g and 22.56 mg Pb/g).

Correlating our results with the results obtained by Chen et al. (2009) it was suggested that the adsorption of strontium increased due to the interaction with calcium hydroxyapatite and this facilitated the ion exchange. Moreover, it is worth noting that the specific surface area and the specific volume of the pores of the BC/CaHA/Sr (Table 1) are higher than that of the pure BC, which can probably improve the accessibility of Sr ions for the material.

#### Effect of pH

The pH of the solution is a key parameter in evaluating the interactions between adsorbate/adsorbent, as it provides information that allows optimization of the conditions for the adsorption system. The adsorbent and adsorbate must be oppositely charged to provide a larger electrostatic interaction between them.

The results in Fig. 9 show that the adsorption capacity was pH-dependent, as there was a reduction in the  $Sr^{2+}$  adsorption when the pH decreased. The lower adsorption in the acidic solutions is attributed to the H<sup>+</sup> ions competing with the metal ions for exchange sites. The higher adsorption for the BC/ CaHA hybrid occurred at pH 6.0. Similar to our result, Nishiyama et al. (2015) also observed the effect of pH on the  $Sr^{2+}$  adsorption in five types of hydroxyapatite materials and found that with increasing pH the absorption also increased, and the highest amount of adsorption was reached at pH 6.0.



1s signals corresponding to a BC, b BC/CaHA, c BC/ CaHA/Sr and d BC/SrAp

Table 3 Surface composition of the studied materials in atomic concentration %

Fig. 6 P 2p and P 2s core level signals of the hybrid materials produced (BC/ CaHA, BC/CaHA/Sr and BC/SrAp)

Samples	С	0	Ca	Р	Sr	Na	Ν	Ca/C	P/C	Sr/C
BC	65.6	33.7	_	_	_	_	_	_	_	_
BC/CaHA	22.5	48.9	11.6	14.2	_	0.4	2.4	0.52	0.63	_
BC/CaHA/Sr	41.0	41.6	6.4	5	0.9	2.5	2.6	0.16	0.12	0.02
BC/SrAp	52.8	34.9	-	2.1	2.3	1.9	2.1	-	0.04	0.04



### Effect of temperature

The temperature is considered to be a limiting factor in an adsorption system. The effect of temperature on the adsorption of Sr ions on the BC/CaHA hybrid was evaluated at 20, 25, 30, and 40 °C.

The adsorption values obtained at the temperatures 20, 25, 30, and 40 °C were 9.59, 17.32, 27.93, and 29.36 mg of Sr per gram of adsorbent, respectively (Fig. 10). Increasing the temperature from 20 to 25 °C lead to an increase of almost 45% of the Sr<sup>2+</sup> adsorbed amount, and from 25 to 30 °C, an increase in adsorption of around 66% was observed. However, when the temperature was increased to 40 °C, only a small additional amount of Sr was adsorbed on the material. This result indicated that 30-40 °C is the optimum temperature range for Sr adsorption on the BC/CaHA hybrid.

Theoretically, the adsorbed amount tends to decrease with increasing temperature, because the adsorption processes are generally exothermic (Doğan et al. 2006) stated that the increase in temperature could trigger a change in pore size, facilitating the

Cellulose (2018) 25:6661-6679

entry of larger adsorbate particles. The results of this study suggest that another phenomenon would likely be occurring along, such as the exchange of cations, which involves ion exchange of calcium from the hydroxyapatite by the strontium present in the solution.

Similar results were found by Saber-Samandari et al. (2013) who studied the potential of cellulosepolyacrylamide hydroxyapatite composites to eliminate copper ions in water treatment. It was found that by increasing the temperature from 20 to 45 °C, the adsorption capacity increased, with the maximum copper uptake achieved at 45 °C, which indicates that the adsorption of  $Cu^{2+}$  by the composite was an endothermic process, favoring a greater movement of the adsorbate to the adsorbent, contributing to ion exchange phenomena.

#### Adsorption isotherm

Adsorption isotherm studies are important to determine the efficacy of adsorption. The equilibrium adsorption isotherm is fundamental to describe the



Fig. 7 Ca 2p, N 1s, Na 1s core level signals of the hybrid materials produced (BC/CaHA, BC/CaHA/Sr and BC/SrAp)

interactive behavior between the adsorbate and adsorbent, and the concentration of adsorbed and dissolved adsorbate at equilibrium. Adsorption equilibrium data have been fitted to the Langmuir model, which is commonly used to describe experimental results in a wide range of concentrations. From the isotherms (Fig. 11), it was noted that the maximum adsorption capacity is directly proportional to the temperature increase.

This isotherm profile is considered favorable to adsorption. The increase in adsorption with increasing

temperature suggests that there is a transition from physical adsorption to chemical adsorption most likely caused by the entropy variations (Sousa et al. 2014).

# Incorporation of SrAp in BC matrix (production of the hybrid BC/SrAp)

As exhibiting in Fig. 12, the total amount of strontium that was incorporated increased after each cycle, although after the third cycle only minor amounts were additionally incorporated as the active sites in the



Fig. 8 Adsorption kinetics of  $Sr^{2+}$  by BC/CaHA as a function of time

matrix were being occupied. The formation of strontium apatite was confirmed due to the reduction in the residual concentration of strontium in the solution. During the alternate soaking of BC in strontium nitrate solution and dibasic sodium phosphate solution, the apatite was formed by chemical precipitation and synthesis of strontium phosphates. When the BC membranes were immersed in SrCl<sub>2</sub> solution at 1000 mg/L, a greater incorporation of Sr was observed, reaching 237.32 mg of Sr per gram of BC after the five cycles, while after five cycles of immersion in SrCl<sub>2</sub> solution at 100 mg/L, an incorporation of 109.54 mg/g of adsorbent was achieved.

The BC/SrAp hybrid material was obtained by chemical precipitation of P and Sr ions with the formation of strontium phosphate on the surface of BC. Therefore, Sr was tightly bound to the material surface, since an ionic bond occurred between the metal and the non-metal surface. Thus, the cellulose matrix containing free hydroxyl (OH<sup>-</sup>) groups



Fig. 9 Effect of pH variation on the adsorption of  $\mathrm{Sr}^{2+}$  on the hybrid BC/CaHA

interacted with  $Sr^{2+}$  (positively charged), forming an ionic bond. At the same time, the phosphate ions  $(PO_4^{3-})$  could bind to the  $Sr^{2+}$ . It has been suggested that during the formation of the BC/SrAp composite, several interactions and intermolecular forces are at play.

NMR analysis confirmed that the BC/SrAp hybrid formed had strontium phosphates chemically bound to bacterial cellulose, indicating chemical adsorption on the material. XPS analysis showed that the formation of strontium phosphates is not similar to that of calcium hydroxyapatite, indicating that strontium delays the formation of the hydroxyapatite phase.

#### Desorption study

From the results presented, it can be observed that for hybrid BC/CaHA/Sr, the condition which lead to higher  $Sr^{2+}$  adsorption (23.02 ± 1.14 mg/g) occurred when the BC membrane was immersed in strontium nitrate solution for 2 h at 40 °C and pH 6. While for the hybrid BC/SrAp, the highest amount of incorporated Sr (237.31 ± 0.42 mg/g) occurred after five immersion cycles in strontium chloride solution at a concentration of 1000 mg/L.

The desorption studies were performed in order to obtain the Sr release profile by the hybrid materials produced at these optimized conditions. The hybrid BC/CaHA/Sr released 6.77 mg/g of Sr after 7 days and 21 mg/g after 120 days (Fig. 13). This faster elution probably indicates that the Sr ions were adsorbed on the BC/CaHA/Sr by physisorption mechanisms. The hybrid BC/SrAp showed a slower release profile than the BC/CaHA/Sr. After 7 days, the



Fig. 10 Effect of temperature on the adsorption of  $\mathrm{Sr}^{2+}$  by BC/ CaHA hybrid

material eluted 6 mg/g of the adsorbed Sr, and after 120 days, only 44 mg/g of Sr was released.

Table 4 shows the Sr release rate per day at different periods during the experiment. On the first day, the release rate was 12.7 and 9.2 mg/g for BC/CaHA/Sr and BC/SrAp, respectively. During the following weeks, the daily release rate decreased for both materials and after 16 weeks (120 days), reached values of 0.004 and 0.06 mg/g per day for BC/CaHA/Sr and BC/SrAp, respectively.

The results indicated that the synthesis route for the production of the BC/SrAp hybrid promoted not only a greater incorporation of Sr into the BC structure, but also produced a material with a slower Sr release profile (retaining about 94% of Sr after 120 days). This slower elution probably indicates that the Sr ions were adsorbed on the BC/SrAp by chemisorption mechanisms. These features make the BC/SrAp a potential material for use in applications where the release of Sr at the implant site should be controlled.

Tiwari et al. (2012) studied drug release mechanisms and found that in order to reach the best therapeutic efficacy, decreased toxicity, and increased time of action, it is important to create systems with a slow release profile (controlled delivery) of active compounds, which ensures a safer administration and lower dosage of the drug. However, in order to combat infections or inflammation, sometimes an initial high dosage is essential, and a large amount of drug must be released quickly at the beginning of the treatment (Vallet-Regí et al. 2007).



**Fig. 11** Adsorption isotherms of  $Sr^{2+}$  (concentration of 10–350 mg/L) on BC/CaHA at pH 6.0 and temperatures of 25 °C ( $\blacksquare$ ) and 40 °C ( $\bigcirc$ )

Energy-dispersive X-ray spectroscopy (EDX)

The MEV/EDX technique was used to verify the surface composition of the samples before and after strontium desorption, in addition to identifying the type of calcium phosphates produced on the surface through the Ca/P ratio.

In the BC/SrAp and BC/CaHA/Sr samples the deposition of the strontium phosphates and calcium phosphates on the surfaces is confirmed (Fig. 14a, c), showing that the immersion cycles method favors the chemical precipitation of hydroxyapatite. After the strontium desorption assay, the percentage of each component present on the surface of these samples was quantified.

Through the micrographs (Fig. 14b, d), it can be seen that after the desorption assay the samples immersed in PBS buffer showed agglomerations on their surface, possibly referring to the salt crystals



Fig. 12 Determination of SrAp incorporation in the BC matrix after each immersion cycle in strontium nitrate solution at concentrations of 100 mg/L (a) and 1000 mg/L (b)

from the buffer itself. In fact, as confirmed by the EDS analysis (Fig. 14b, d), there was a significant increase in the amount of elements such as Na and Cl in the samples after the desorption assay.

In the sample BC/SrAp (Fig. 14a), elements such as oxygen and carbon were detected by EDS, which are typical of the cellulose structure. On the other hand, the phosphorus and strontium detected came from the chemical precipitation step during the deposition of strontium apatite on BC fibres. The major component (41.7%) found in BC/SrAp sample before the desorption study was Sr. Meanwhile, after the desorption assay, only 13.2% of Sr was found on the sample surface (Fig. 14b), confirming the release of strontium.

In BC/CaHA/Sr samples (Fig. 14c) the followings elements were detected: oxygen, carbon, phosphorus and strontium, a high amount (38%) of calcium and traces of sodium and chlorine. The stoichiometric ratio of 2.27 Ca/P, which suggests that the hydroxyapatite deposited on the material are tetracalcium phosphates. The strontium content (4%) was well below that of calcium, probably because Sr was incorporated by physical adsorption, where it had to compete by the active sites with the calcium already present on the surface.

When the BC/CaHA/Sr sample was submitted to the desorption assay, the calcium contents decreased and the sodium and chlorine contents increased. Only traces of strontium were found, confirming that this element was desorbed throughout the days (Fig. 14d). The traces of aluminium detected are likely to come from contamination during preparation of the samples for analysis.

#### Conclusions

This work describes for the first time the production of hybrids based on bacterial cellulose and hydroxyapatite as a controlled strontium delivery systems, favoring biomaterial research aimed at future applications in guided bone regeneration.

Bacterial cellulose/hydroxyapatite hybrid materials were produced via two routes of synthesis. These materials are able to incorporate strontium through distinct adsorption/desorption profiles for each material that involved physisorption and chemisorption mechanisms.

![](_page_15_Figure_10.jpeg)

Fig. 13 Strontium desorption from the hybrid materials at optimized conditions observed for a duration of 120 days. Circle markers (BC/SrAp  $\bullet$ ) and Square markers (BC/CaHA/Sr  $\blacksquare$ ). The small graphic reports the Sr<sup>2+</sup> desorption during the first 5 h of the experiment. The arrows indicate that after 120 days, the percentages of Sr desorbed were 6 and 91% for BC/SrAp and BC/CaHA/Sr, respectively

The BC/SrAp material exhibited increases strontium adsorption capacity and its release was slow and controlled because of the strong chemical bond formed between the metal and the cellulose matrix/ hydroxyapatite, ensuring controlled doses for a period of over 4 months. Hence, this material is a promising strontium delivery system to assist bone-remodeling mechanism during GBR therapeutic protocol. Subsequently, in vivo studies are required to evaluate the

**Table 4** Strontium release rate/day from hybrid materialsstudied for a duration of 16 weeks (120 days)

Period	Release rate/day (mg/g) <sup>a</sup>		
	BC/CaHA/Sr	BC/SrAp	
1st day	12.7	9.2	
1st week	1.13	0.99	
2nd week	0.14	0.95	
3rd week	0.07	0.7	
4–6th week	0.03	0.4	
7–16th week	0.004	0.06	

<sup>a</sup>Average amount of strontium released per day during the indicated period

![](_page_16_Figure_2.jpeg)

Fig. 14 Electron micrographs and energy-dispersive X-ray spectroscopy of the surfaces of **a**, **b** BC/SrAp and **c**, **d** BC/CaHA/Sr, before (**a** and **c**) and after (**b** and **d**) the desorption of Sr

biocompatibility and the therapeutic efficacy of the materials produced.

Acknowledgments The authors would like to thank the Coordination for the Improvement of Higher Education Personnel (CAPES), National Counsel of Technological and Scientific Development (CNPq), Cearense Foundation for the Support of Scientific and Technological Development (FUNCAP), and the Embrapa Agroindústria Tropical for funding this research. This research was also supported by the following projects: FUNCAP/CNPq (PR2-0101-00023.01.00/ 305504/2016-9), PROCAD/CAPES 15), CNPq (No. (88881.068439/2014-01) and CTQ2015-68951-C3-3R (Ministerio de Economía y Competitividad, Spain and FEDER Funds). A.I.M. thanks the Ministry of Economy and Competitiveness for a Ramón y Cajal contract (RyC2015-17870).

#### References

- Ahn SJ et al (2015) Characterization of hydroxyapatite-coated bacterial cellulose scaffold for bone tissue engineering. Biotechnol Bioprocess Eng 20:948–955. https://doi.org/10. 1007/s12257-015-0176-z
- Bhatnagar VM (1967) Infrared spectrum of strontium hydroxyapatit. Experientia 23:697–699. https://doi.org/10.1007/ bf02154118
- Brunauer S, Emmett PH, Teller E (1938) Adsorption of gases in multimolecular layers. J Am Chem Soc 60:309–319. https://doi.org/10.1021/ja01269a023
- Cacicedo ML et al (2016) Modified bacterial cellulose scaffolds for localized doxorubicin release in human colorectal HT-29 cells. Colloids Surf B 140:421–429. https://doi.org/10. 1016/j.colsurfb.2016.01.007
- Capitani D, Crescenzi V, De Angelis AA, Segre AL (2001) Water in hydrogels. an nmr study of water/polymer interactions in weakly cross-linked chitosan networks. Macromolecules 34:4136–4144. https://doi.org/10.1021/ ma002109x

- Ceratti DR et al (2015) Critical effect of pore characteristics on capillary infiltration in mesoporous films. Nanoscale 7:5371–5382. https://doi.org/10.1039/c4nr03021d
- Chen S et al (2009) Carboxymethylated-bacterial cellulose for copper and lead ion removal. J Hazard Mater 161:1355–1359. https://doi.org/10.1016/j.jhazmat.2008. 04.098
- Chen Y et al (2012) Role of calcium in metalloenzymes: effects of calcium removal on the axial ligation geometry and magnetic properties of the catalytic diheme center in MauG. Biochemistry 51:1586–1597. https://doi.org/10. 1021/bi201575f
- Doğan M et al (2006) Adsorption kinetics of maxilon blue GRL onto sepiolite from aqueous solutions. Chem Eng. J 124:89–101. https://doi.org/10.1016/j.cej.2006.08.016
- Dolinina ES et al (2017) Effect of trehalose on structural state of bovine serum albumin adsorbed onto mesoporous silica and the protein release kinetics in vitro. Colloids Surf A 527:101–108. https://doi.org/10.1016/j.colsurfa.2017.05. 014
- Duarte EB et al (2015) Production of hydroxyapatite-bacterial cellulose nanocomposites from agroindustrial wastes. Cellulose 22:3177–3187. https://doi.org/10.1007/s10570-015-0734-8
- Dufresne A (2012) Nanocellulose: from nature to high performance tailored materials. E-book. Walter de Gruyter, Berlin
- Foresti ML, Vázquez A, Boury B (2017) Applications of bacterial cellulose as precursor of carbon and composites with metal oxide, metal sulfide and metal nanoparticles: a review of recent advances. Carbohydr Polym 157:447–467. https://doi.org/10.1016/j.carbpol.2016.09. 008
- Gea S et al (2011) Investigation into the structural, morphological, mechanical and thermal behaviour of bacterial cellulose after a two-step purification process. Bioresour Technol 102:9105–9110. https://doi.org/10.1016/j. biortech.2011.04.077
- Grande CJ et al (2009) Nanocomposites of bacterial cellulose/ hydroxyapatite for biomedical applications. Acta Biomater 5:1605–1615. https://doi.org/10.1016/j.actbio.2009.01.022
- Heinze T, Liebert T, Koschella A (2014) Esterification of polysaccharides. Springer, Berlin
- Henderson CMB et al (2016) X-ray absorption study of 3d transition-metals and Mg in glasses and analogue crystalline materials in A Fe 3 + Si 2 O 6 and A 2 X 2 + Si 5 O 12, where A = K, Rb, or Cs and X = Mg, Mn, Fe Co, Ni, Cu, or Zn. J Non-Cryst Solids 451:23–48. https://doi.org/10.1016/j.jnoncrysol.2016.05.016
- Hestrin S, Schramm M (1954) Synthesis of cellulose by *Ace-tobacte rxylinum*. Preparation of freeze-dried cells capable of polymerizing glucose to cellulose. Biochem J 58:345–352
- Hidalgo-Carrillo J et al (2010) A study on the potential application of natural phosphate in photocatalytic processes. J Colloid Interface Sci 344:475–481. https://doi.org/10. 1016/j.jcis.2010.01.020
- Hidalgo-Carrillo J et al (2012) XPS evidence for structureperformance relationship in selective hydrogenation of crotonaldehyde to crotyl alcohol on platinum systems

supported on natural phosphates. J Colloid Interface Sci 382:67–73. https://doi.org/10.1016/j.jcis.2012.05.050

- Hing KA (2005) Bioceramic bone graft substitutes: influence of porosity and chemistry. Int J App Ceram Technol 2:184–199. https://doi.org/10.1111/j.1744-7402.2005. 02020.x
- Hutchens S (2007). Characterization of a biomimetic calciumdeficient hydroxyapatite-bacterial cellulose composite. Ph.D. Dissertation, University of Tennessee
- Hutchens S et al (2006) Biomimetic synthesis of calcium-deficient hydroxyapatite in a natural hydrogel. Biomaterials 27:4661–4670. https://doi.org/10.1016/j.biomaterials. 2006.04.032
- Ide-Ektessabi A, Yamaguchi T, Tanaka Y (2005) RBS and XPS analyses of the composite calcium phosphate coatings for biomedical applications. Nucl Instrum Methods Phys Res B 241:685–688. https://doi.org/10.1016/j.nimb.2005.07. 165
- Khiari R et al (2017) Synthesis and characterization of cellulose carbonate using greenchemistry: surface modification of Avicel. Carbohyd Polym 163:254–260. https://doi.org/10. 1016/j.carbpol.2017.01.037
- Lin KSK et al (2005) Mechanistic study of apatite formation on bioactive glass surface using31P solid-state NMR spectroscopy. Chem Mater 17:4493–4501. https://doi.org/10. 1021/cm050654c
- Liu Y et al (2005) Crosslinked organic-inorganic hybrid chitosan membranes for pervaporation dehydration of isopropanol-water mixtures with a long-term stability. J Membr Sci 251:233–238. https://doi.org/10.1016/j. memsci.2004.12.003
- Marie PJ, Felsenberg D, Brandi ML (2010) How strontium ranelate, via opposite effects on bone resorption and formation, prevents osteoporosis. Osteoporos Int 22:1659–1667. https://doi.org/10.1007/s00198-010-1369-0
- Melnikov P, Gonçalves RV (2015) Preparation and characterization of strontium hydroxyapatite Sr10(PO<sub>4</sub>)6(-OH)2·10H2O suitable for orthopedic applications. Mater Lett 150:89–92. https://doi.org/10.1016/j.matlet.2015.02. 110
- Nishiyama Y et al (2015) Adsorption and removal of strontium in aqueous solution by synthetic hydroxyapatite. J Radioanal Nucl Chem 307:1279–1285. https://doi.org/10. 1007/s10967-015-4228-9
- Ohtsu N, Nakamura Y, Semboshi S (2012) Thin hydroxyapatite coating on titanium fabricated by chemical coating process using calcium phosphate slurry. Surf Coat Technol 206:2616–2621. https://doi.org/10.1016/j.surfcoat.2011. 11.022
- Pan HB et al (2009) Solubility of strontium-substituted apatite by solid titration. Acta Biomater 5:1678–1685. https://doi. org/10.1016/j.actbio.2008.11.032
- Pértile RAN et al (2012) Bacterial cellulose: long-term biocompatibility studies. J Biomater Sci Polym 23:1–16. https://doi.org/10.1163/092050611x581516
- Pigossi SC et al (2015) Bacterial cellulose-hydroxyapatite composites with osteogenic growth peptide (OGP) or pentapeptide OGP on bone regeneration in critical-size calvarial defect model. J Biomed Mater Res 103:3397–3406. https://doi.org/10.1002/jbm.a.35472

- Querido W, Rossi AL, Farina M (2016) The effects of strontium on bone mineral: a review on current knowledge and microanalytical approaches. Micron 80:122–134. https:// doi.org/10.1016/j.micron.2015.10.006
- Rad MM et al (2017) Fabrication and characterization of twolayered nanofibrous membrane for guided bone and tissue regeneration application. Mater Sci Eng C 80:75–87. https://doi.org/10.1016/j.msec.2017.05.125
- Rajwade JM, Paknikar KM, Kumbhar JV (2015) Applications of bacterial cellulose and its composites in biomedicine. Appl Microbiol Biotechnol 99:2491–2511. https://doi.org/10. 1007/s00253-015-6426-3
- Rakhmatia YD et al (2013) Current barrier membranes: titanium mesh and other membranes for guided bone regeneration in dental applications. J Prosthodont Res 57:3–14. https://doi. org/10.1016/j.jpor.2012.12.001
- Rehman I, Bonfield W (1997) Characterization of hydroxyapatite and carbonated apatite by photo acoustic FTIR spectroscopy. J Mater Sci Mater Med 8:1–4. https://doi.org/10. 1023/a:1018570213546
- Retzepi M, Donos N (2010) Guided bone regeneration: biological principle and therapeutic applications. Clin Oral Implants Res 21:567–576. https://doi.org/10.1111/j.1600-0501.2010.01922.x
- Saber-Samandari S, Saber-Samandari S, Gazi M (2013) Cellulose-graft-polyacrylamide/hydroxyapatite composite hydrogel with possible application in removal of Cu (II) ions. React Funct Polym 73:1523–1530. https://doi.org/10. 1016/j.reactfunctpolym.2013.07.007
- Saska S et al (2011) Bacterial cellulose-hydroxyapatite nanocomposites for bone regeneration. Int J Biomater 2011:1–8. https://doi.org/10.1155/2011/175362
- Schumacher M et al (2016) Strontium substitution in apatitic CaP cements effectively attenuates osteoclastic resorption but does not inhibit osteoclastogenesis. Acta Biomater 37:184–194. https://doi.org/10.1016/j.actbio.2016.04.016
- Shpak AP, Karbovskii VL, Vakhney AG (2004) Electronic structure of isomorphically substituted strontium apatite. J Electron Spectrosc Relat Phenom 137–140:585–589. https://doi.org/10.1016/j.elspec.2004.02.056
- Sousa RCS et al (2014) Adsorption of alpha-lactalbumin from milk whey on hydroxyapatite: effect of ph and temperature and thermodynamic analysis. Quím Nova 37:950–955. https://doi.org/10.5935/0100-4042.20140149
- Sugiyama S (2003) Enhancement of the catalytic activities in propane oxidation and H-D exchangeability of hydroxyl groups by the incorporation with cobalt into strontium

hydroxyapatite. J Catal 214:8–14. https://doi.org/10.1016/ s0021-9517(02)00101-x

- Swift P (1982) Adventitious carbon-the panacea for energy referencing? Surf Interface Anal 4:47–51. https://doi.org/ 10.1002/sia.740040204
- Tiwari G et al (2012) Drug delivery systems: an updated review. Int J Pharma Investig 2:2–11. https://doi.org/10.4103/ 2230-973x.96920
- Ummartyotin S, Thiangtham S, Manuspiya H (2017) Strontiummodified bacterial cellulose and a polyvinylidene fluoride composite as an electroactive material. For Prod J 67:288–296. https://doi.org/10.13073/fpj-d-16-00041
- Vallet-Regí M, Ruiz-Hernández E (2011) Bioceramics: from bone regeneration to cancer nanomedicine. Adv Mater 23:5177–5218. https://doi.org/10.1002/adma.201101586
- Vallet-Regí M, Balas F, Arcos D (2007) Mesoporous materials for drug delivery. Angew Chem Int Ed 46:7548–7558. https://doi.org/10.1002/anie.200604488
- Venugopal A, Scurrell MS (2003) Hydroxyapatite as a novel support for gold and ruthenium catalysts behaviour in the water gas shift reaction. Appl Catal 245:137–147. https:// doi.org/10.1016/s0926-860x(02)00647-6
- Wang X et al (2009) Towards predicting Ca2 + -binding sites with different coordination numbers in proteins with atomic resolution. Proteins Struct Funct Bioinform 75:787–798. https://doi.org/10.1002/prot.22285
- Yukhnevich GV (1973) Infrared spectroscopy of water. Nauka, Moscow
- Zeng X, Ruckenstein E (1996) Control of pore sizes in macroporous chitosan and chitin membranes. Ind Eng Chem Res 35:4169–4175. https://doi.org/10.1021/ie960270j
- Zhang W et al (2011) Effects of strontium in modified biomaterials. Acta Biomater 7:800–808. https://doi.org/10.1016/ j.actbio.2010.08.031
- Zhang H et al (2014) Universal influenza vaccines, a dream to be realized soon. Viruses 6:1974–1991. https://doi.org/10. 3390/v6051974
- Zhong LR et al (2013) Nitric oxide regulates neuronal activity via calcium-activated potassium channels. PLoS ONE 8:1–12. https://doi.org/10.1371/journal.pone.0078727
- Zhou Y et al (2012) Probing Ca2 + -binding capability of viral proteins with the EF-hand motif by grafting approach. Methods Mol Biol 963:37–53. https://doi.org/10.1007/978-1-62703-230-8\_3
- Zimmermann KA et al (2011) Biomimetic design of a bacterial cellulose/hydroxyapatite nanocomposite for bone healing applications. Mater Sci Eng C 31:43–49. https://doi.org/10. 1016/j.msec.2009.10.007